



# Optimal design of detector thickness for dual-energy x-ray imaging

@2016 KNS spring meeting

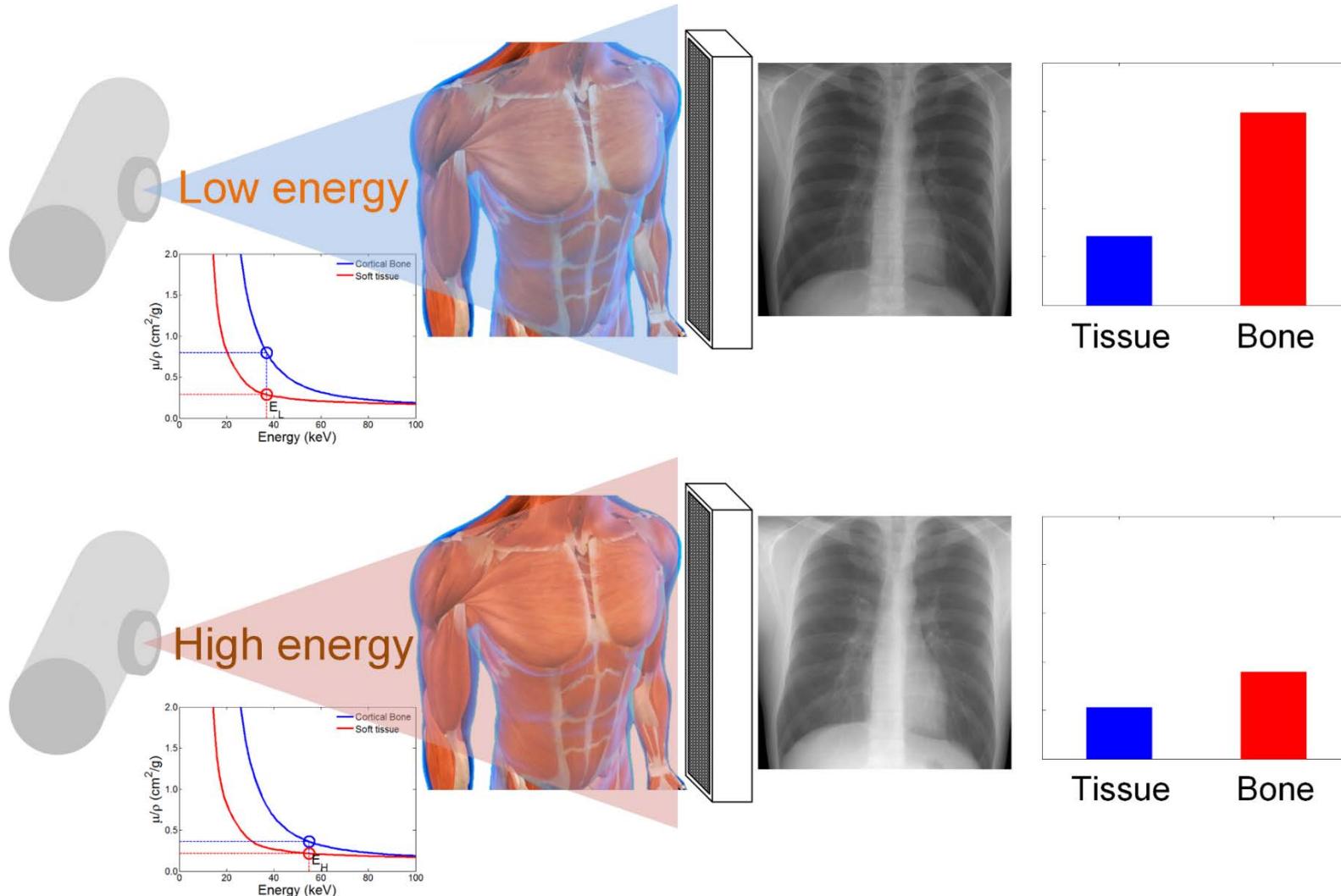
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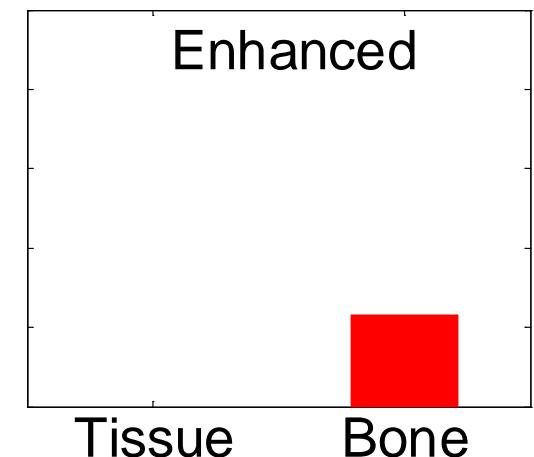
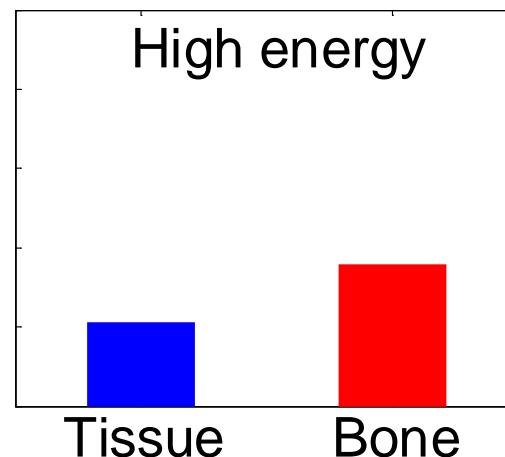
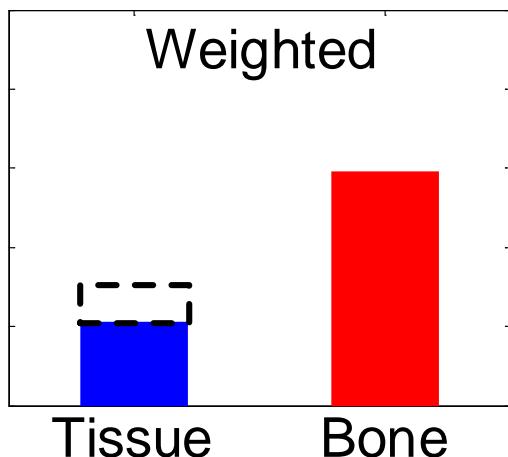
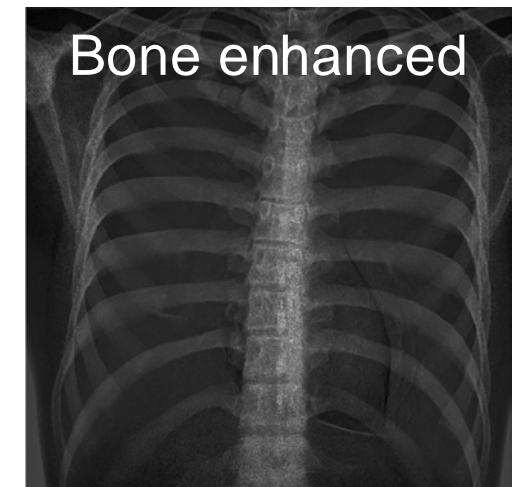
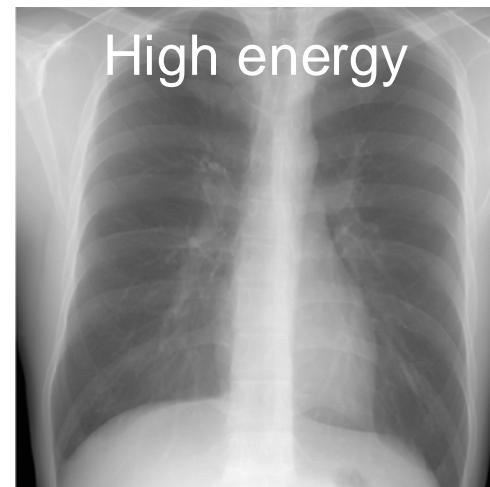
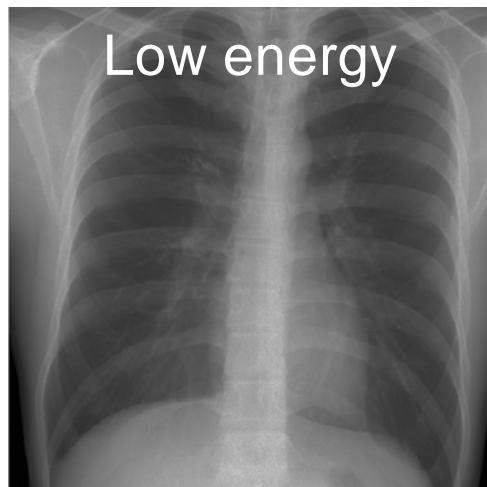
# Outline

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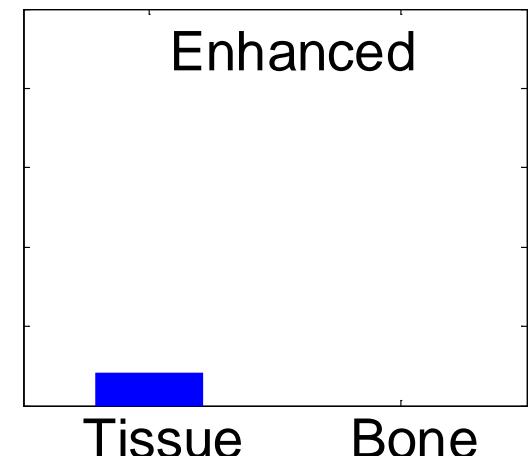
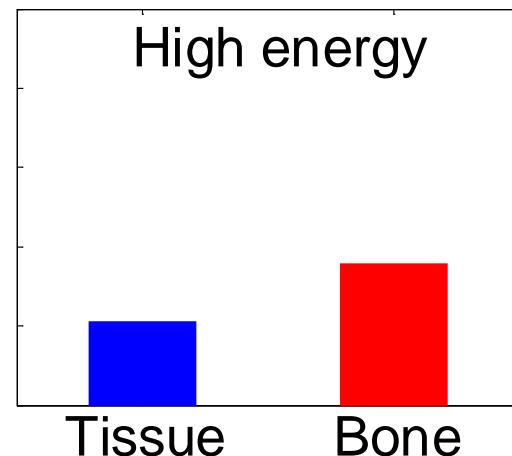
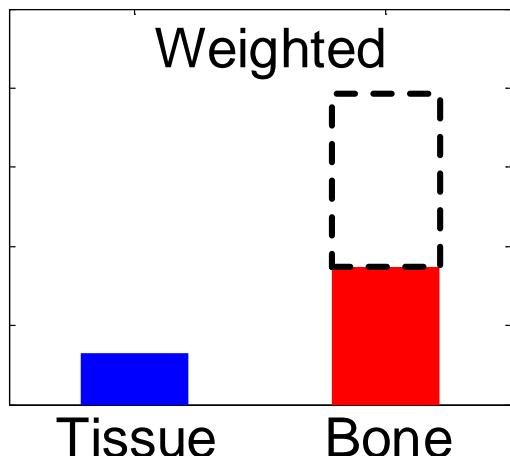
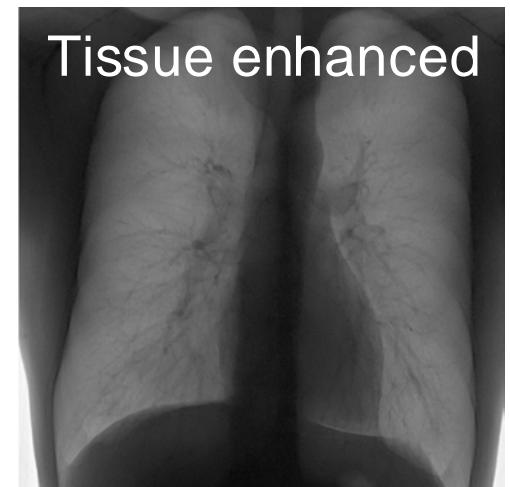
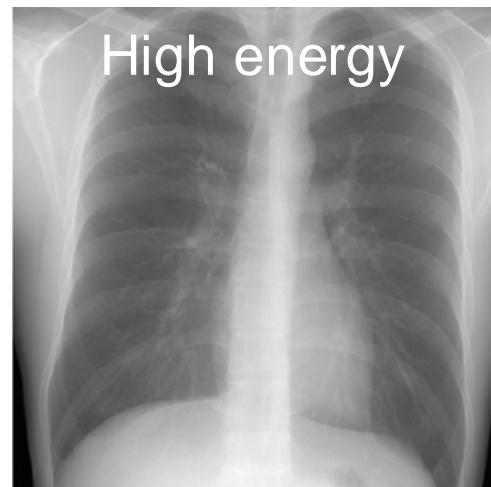
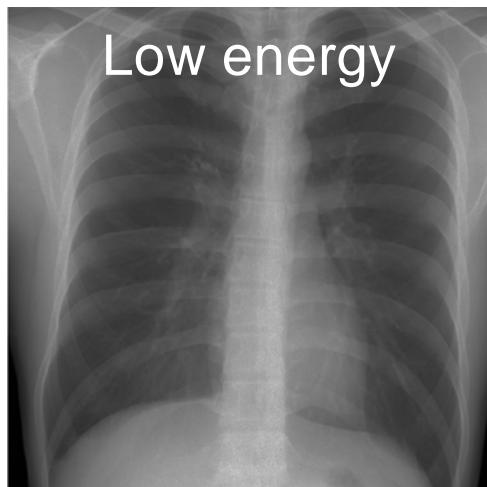
# Dual-energy imaging



# Dual-energy imaging

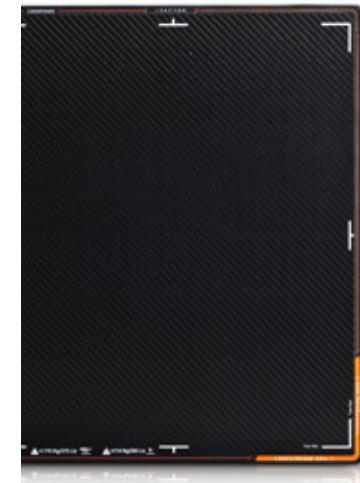


# Dual-energy imaging



# Motivation

- Commercial dual “single” of flat-



GE Healthcare

CsI:Tl

200 mg/cm<sup>2</sup>

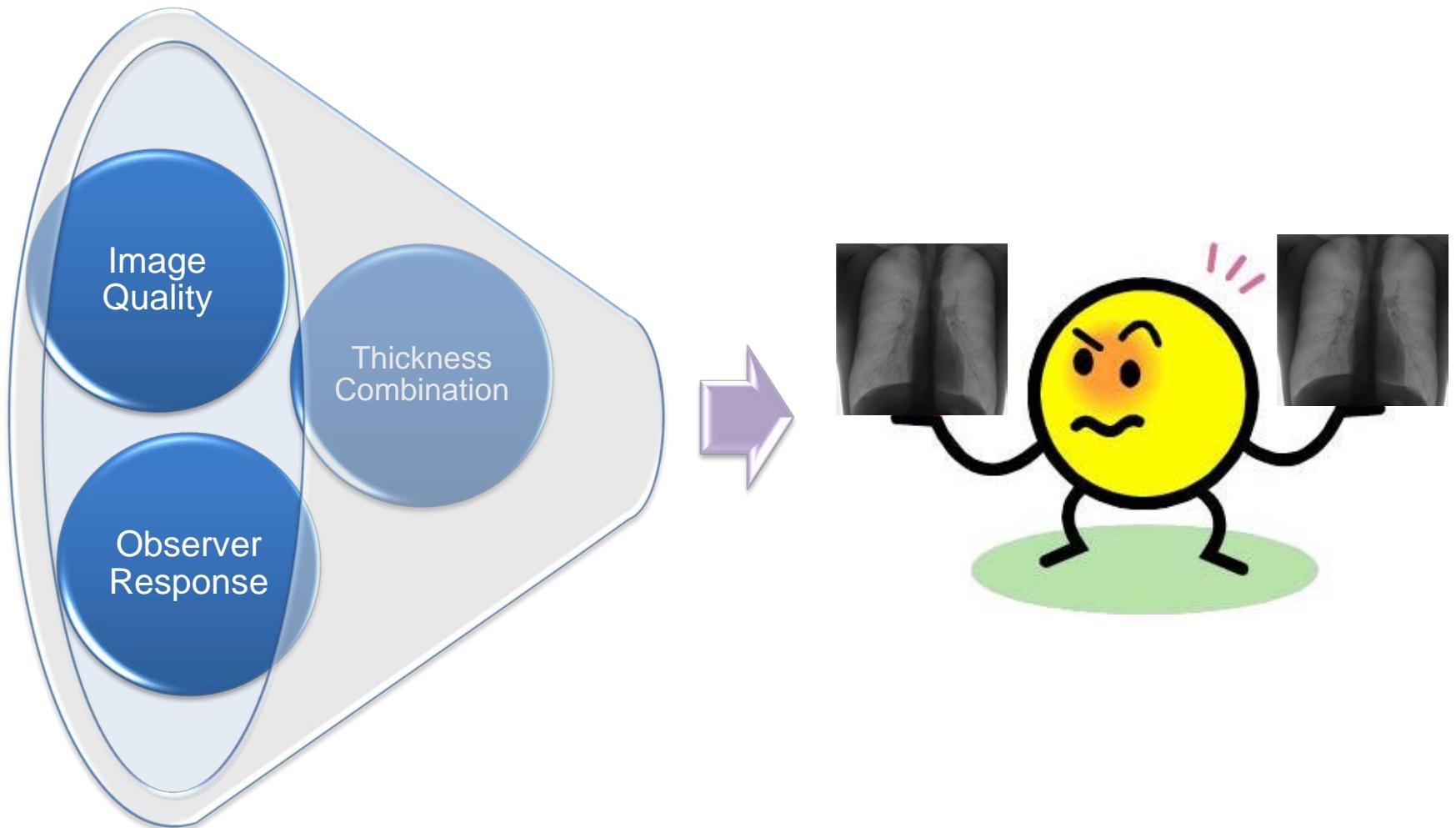
N. W. Marshall et al., “Quality control measurements for digital x-ray detectors,” Phys. Med. Biol., Vol. 56, pp. 979-999, 2011

Radiation Imaging Laboratory,

Pusan National University

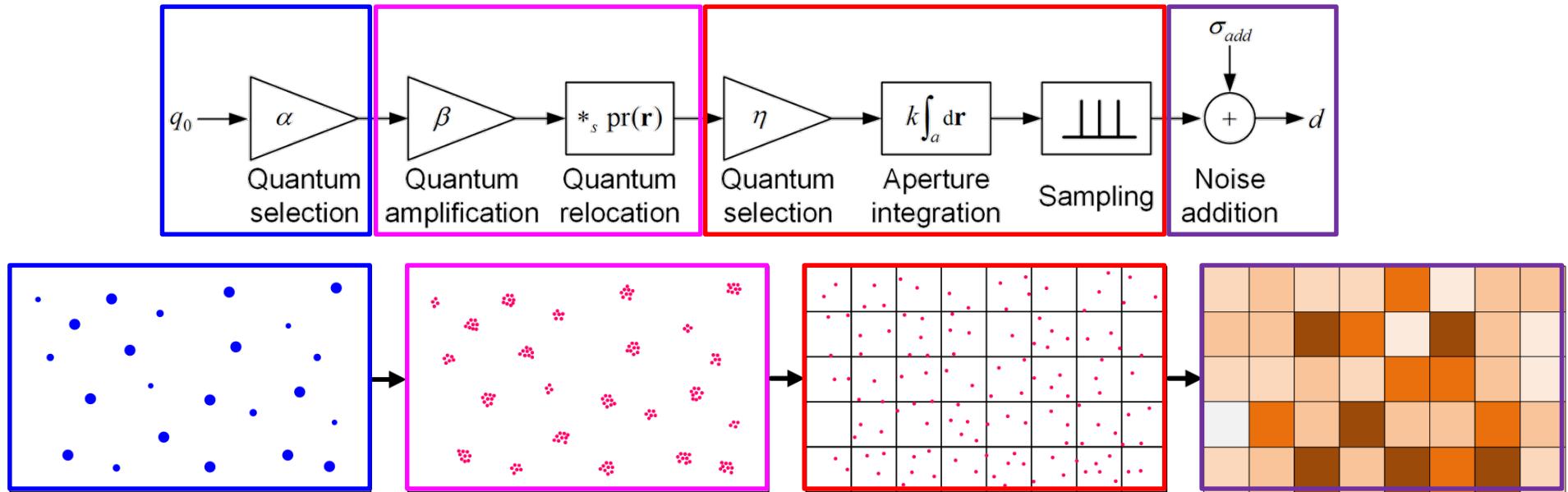
Dong Woon Kim {dongwoonkim@pusan.ac.kr}

# Strategy



# Modeling

- A simple cascaded-systems model describing the signal and noise propagation in an indirect flat-panel detector



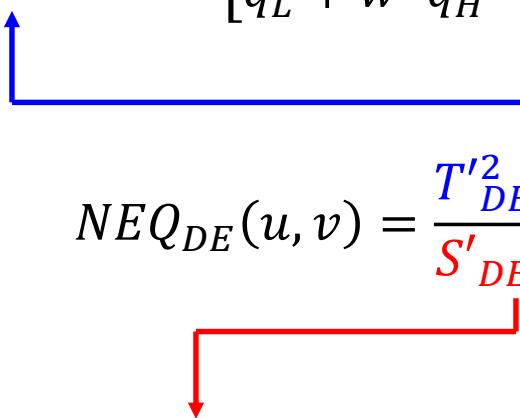
$$S'(u, v) = \frac{1}{\bar{q}_0} \left[ \frac{1}{\gamma \bar{g}} + \frac{\sum_{i=0}^{\infty} \sum_{j=0}^{\infty} T^2 \left( u \pm \frac{i}{p}, v \pm \frac{j}{p} \right)}{\alpha} \left( \frac{1}{I} - \frac{1}{\beta} \right) \right] + \frac{p^2 \sigma_{add}^2}{\bar{q}_0 \bar{g}^2}$$

$$NEQ(u, v) = \frac{T^2(u, v)}{S'(u, v)}$$

# Modeling

- The DQE in DE images may be expressed in the conventional DQE form:

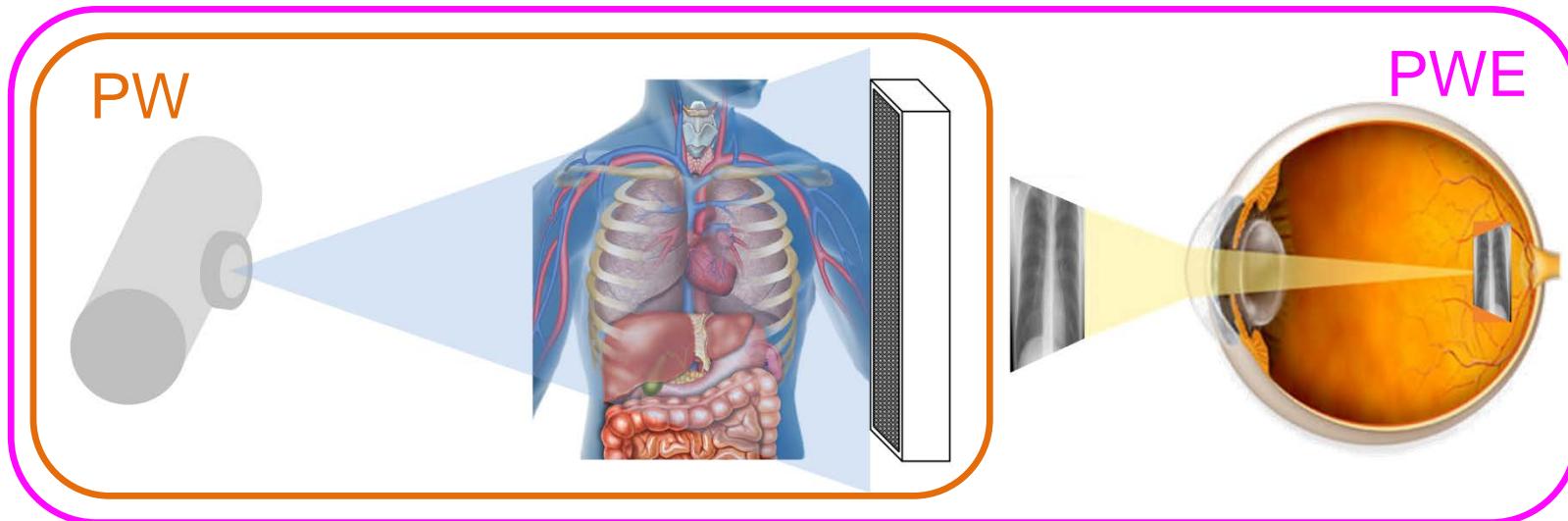
$$T'_{DE}(u, v) = \left[ \frac{w^2 \bar{q}_H}{\bar{q}_L + w^2 \bar{q}_H} T_L^2(u, v) + \frac{\bar{q}_L}{\bar{q}_L + w^2 \bar{q}_H} T_H^2(u, v) \right]^{1/2}$$



$$NEQ_{DE}(u, v) = \frac{T'^2_{DE}(u, v)}{S'_{DE}(u, v)}$$

$$S'_{DE}(u, v) = w^2 S'_L(u, v) + S'_H(u, v)$$

# Detectability index



- Detectability index for the prewhitening matched filter observer model

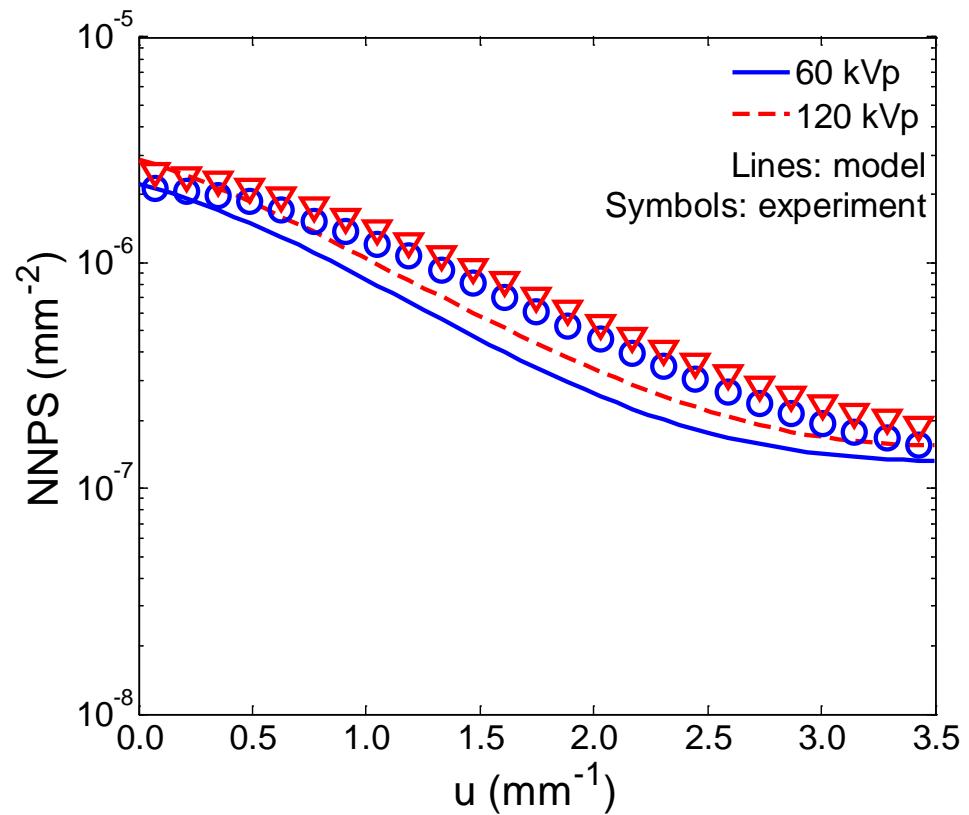
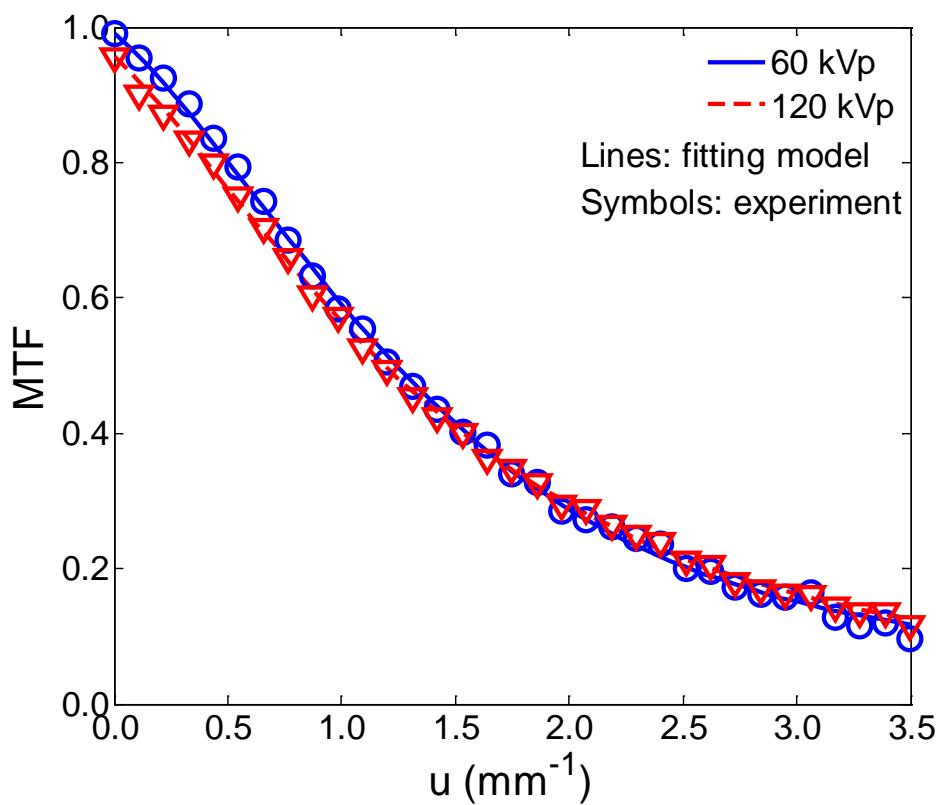
$$d'_{PW} = \iint \frac{\{T^2(u, v)W(u, v)\}}{S'(u, v)} dudv$$

- To include a human eye filter and internal noise

$$d'_{PWE} = \iint \frac{E^2(u, v)\{T^2(u, v)W(u, v)\}}{E^2(u, v)S'(u, v) + N_{int}} dudv$$

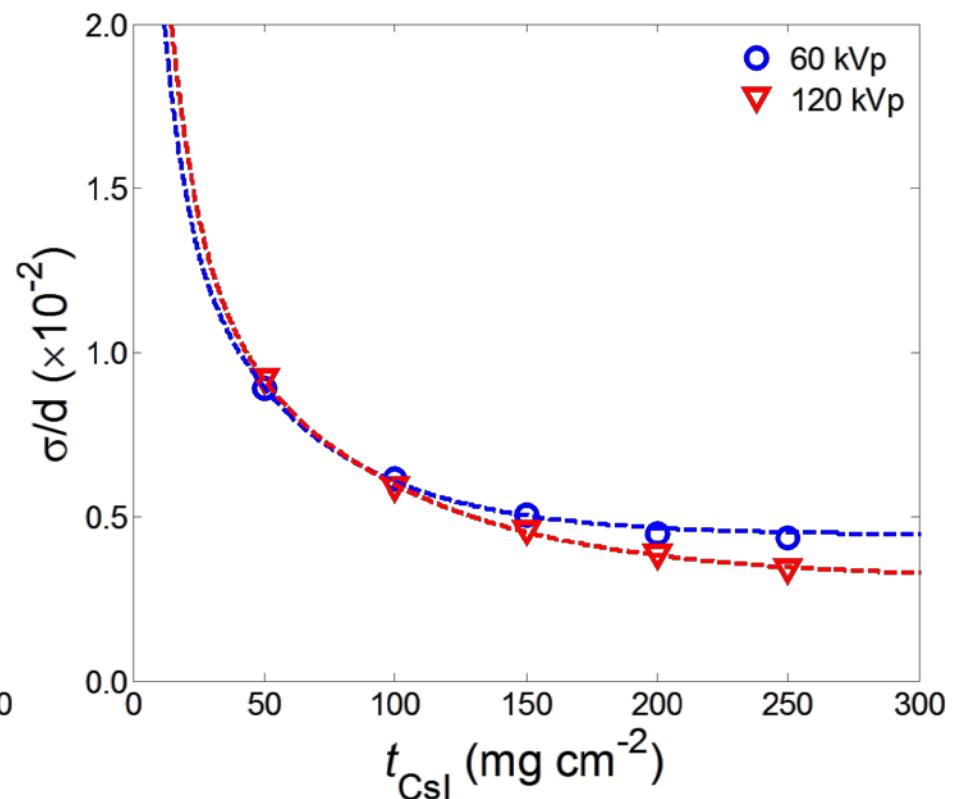
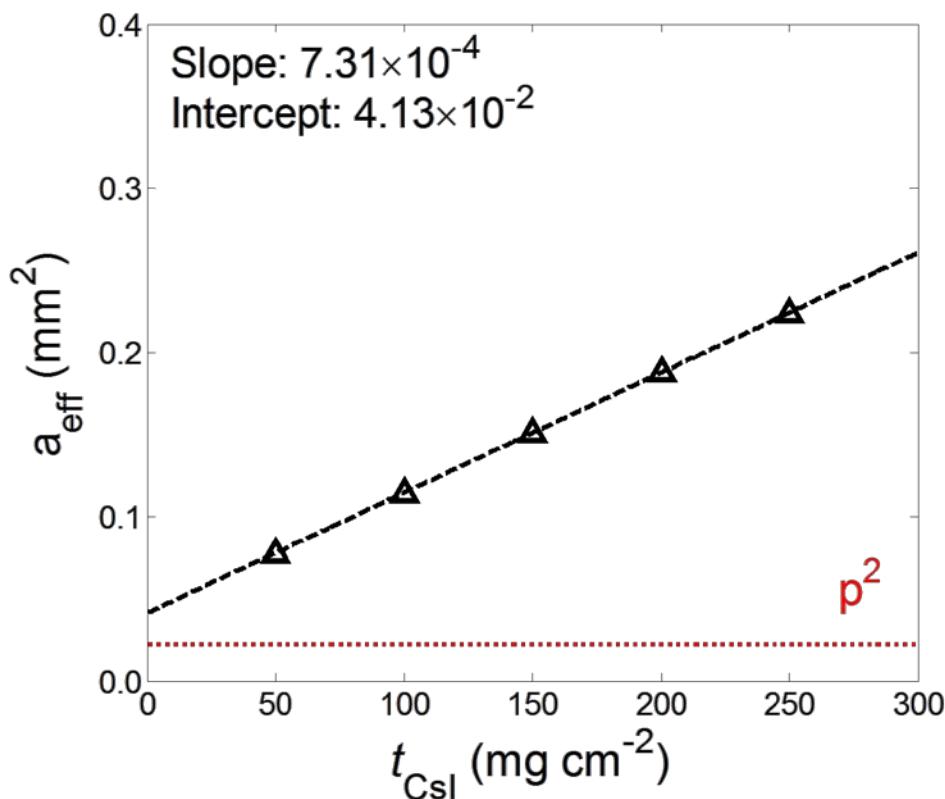
# Validation

- Validation between measured in CsI/a-Si detector and CSA model
- 60 kVp + (13.5 + 2.5) mmAl / 120 kVp + (23.0 + 4.5) mmAl + 0.3 mmCu



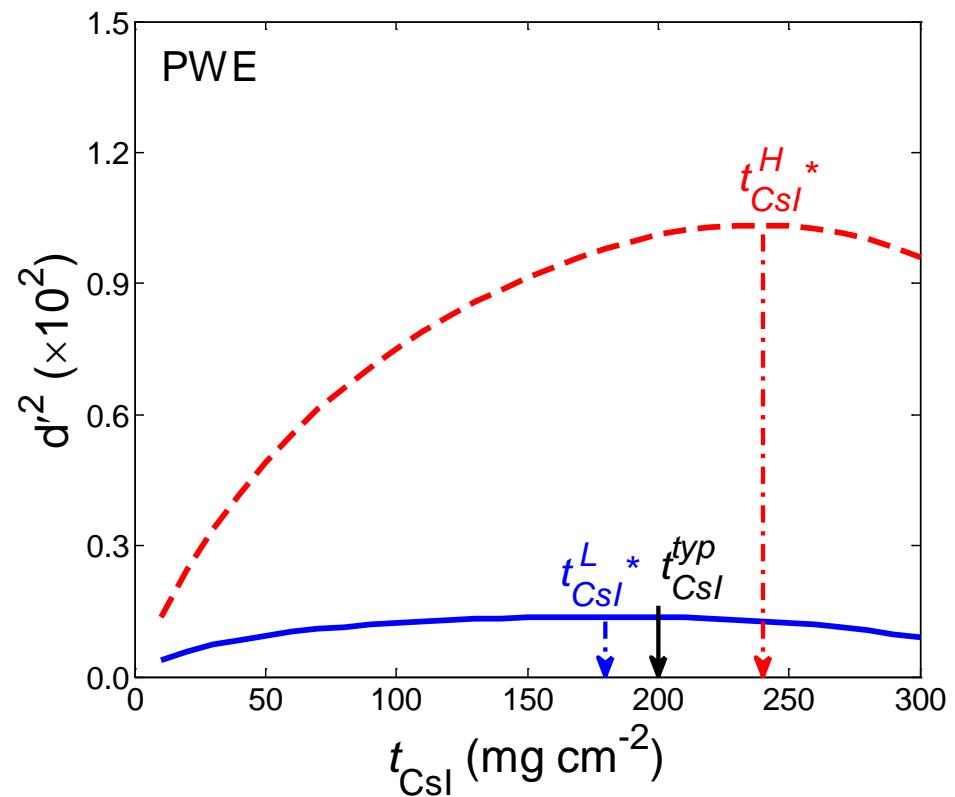
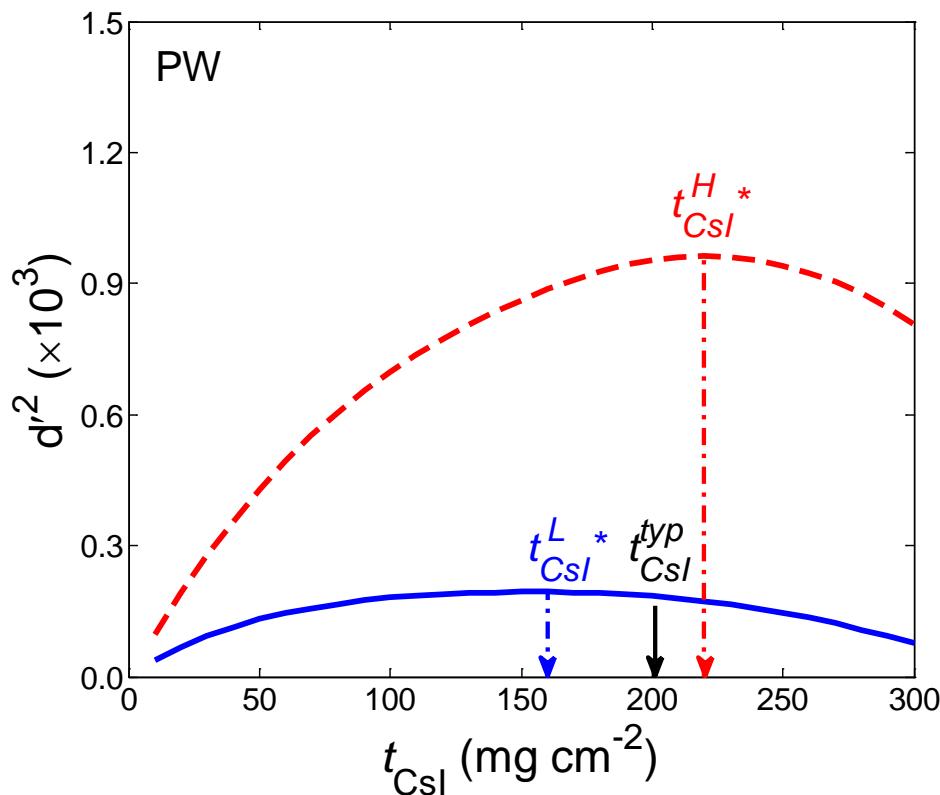
# Theoretical performance

- Calculation results of hypothetical detector performances using the cascaded-systems model
  - $a_{eff} = [2\pi \int_0^\infty T(f)df]^{-1}$ ,  $\sigma/d \sim (\bar{q}_0 a_{eff} \alpha I)^{-1/2}$



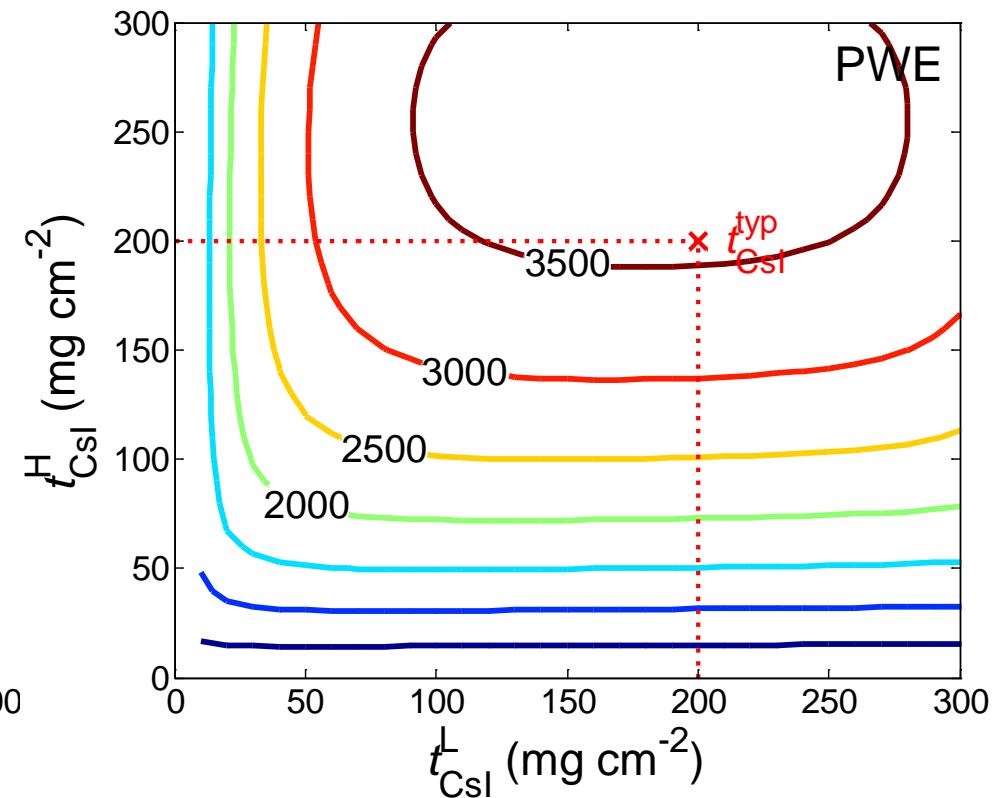
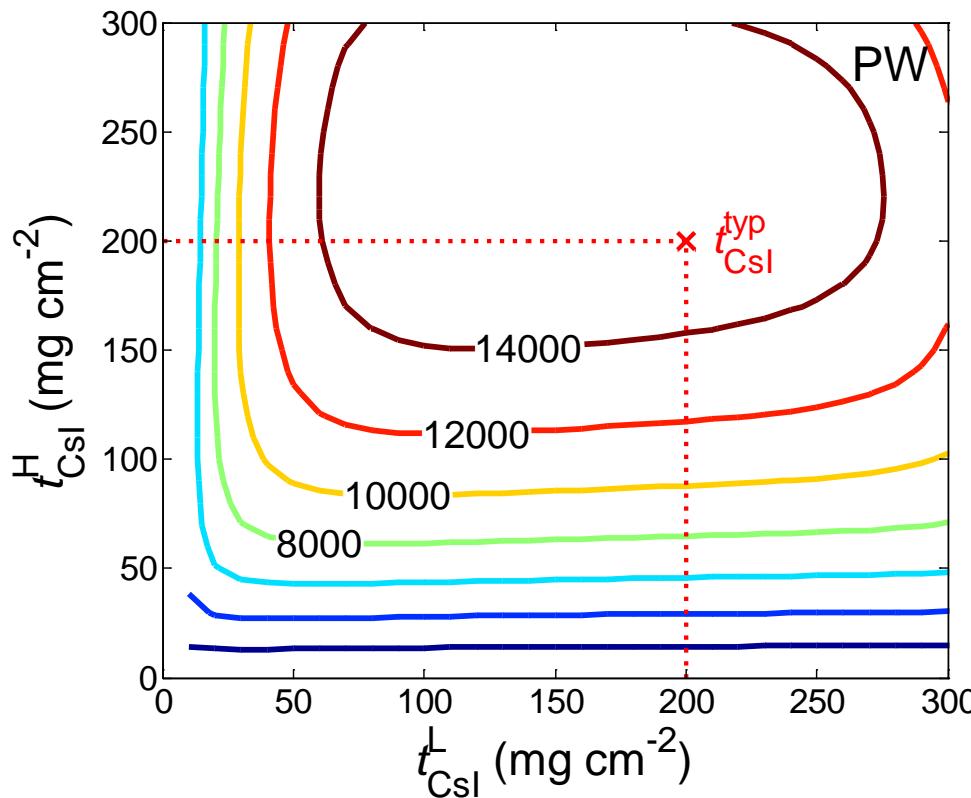
# Detectability index

- Detectability indexes of conventional radiography
  - In the detectability index for the PW model, the typical CsI thickness (i.e.,  $t_{CsI}^{typ} = 200 \text{ mg cm}^{-2}$ ) is located between the respective optimal CsI thicknesses calculated for low and high-kVp spectra



# Detectability index

- Detectability indexes of dual-energy radiography
  - For the PW model, the optimal  $t_{CsI}^H$  for dual-energy imaging ranges  $\sim 120 - 250 \text{ mg cm}^{-2}$  for the low-kVp spectrum whereas it ranges for  $\sim 230 - 300 \text{ mg cm}^{-2}$  or thicker for the high-kVp spectrum



# Conclusion

- The optimal CsI thickness for dual-energy chest imaging has been theoretically investigated by evaluating prewhitening observer model detectability indexes
- To evaluate the PW and PWE detectability indexes, dual-energy fluence and MTF have been reviewed compared to the conventional descriptions
- From the calculation results, the typical CsI thickness of  $200 \text{ mg cm}^{-2}$  is placed in the optimal extent with the PWE model, whereas the PW model requires a larger CsI thickness for better detectability performance
- Although  $t_{CsI}^{typ}$  does not much depart from the optimal ranges, the  $t_{CsI}$  larger than  $t_{CsI}^{typ}$  is preferred for a better dual-energy imaging performance
- It is worth to note that **the absolute values of detectability indexes obtained for dual-energy radiography are higher than those for conventional radiography**

# Detectability index

